PATTERN SWITCHING IN HUMAN MULTILIMB COORDINATION DYNAMICS

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A relative phase model of four coupled oscillators is used to interpret experiments on the coordination between rhythmically moving human limbs. The pairwise coupling functions in the model are motivated by experiments on two-limb coordination. Stable patterns of coordination between the limbs are represented by fixed points in relative phase coordinates. Four invariant circles exist in the model, each containing two patterns of coordination seen experimentally. The direction of switches between two four-limb patterns on the same circle can be understood in terms of two-limb coordination. Transitions between patterns in the human four-limb system are theoretically interpreted as bifurcations in a nonlinear dynamical system.

1. Introduction. In the study of biological motor control a primary question is how spatiotemporal patterns (e.g. locomotory patterns) form in systems composed of a large number of components. Theoretically the question is whether their behavior can be described by a few well-chosen state variables, no matter the number of components involved. For example, the behavioral patterns found between two rhythmically moving fingers have been characterized by a single state variable, the relative phase between the fingers (Kelso, 1984). This low-dimensional description was motivated by the assumption that the movement of each finger reflects the output of a distinct oscillator (Haken et al., 1985). From this viewpoint, the coordination between fingers arises from the interactions between two coupled oscillators. Under general assumptions, when oscillators are weakly coupled,
their dynamics are well approximated by a function of their relative phases (Cohen et al., 1982; Ermentrout and Kopell, 1984). Such a relative phase description is also valid in certain cases of strongly coupled oscillators (Ermentrout and Kopell, 1991).

Applying the same approach as above, Schöner et al. (1990) proposed a model of quadruped locomotion, using three relative phases as state variables. Assuming left–right and front–hind symmetry they analysed the stability of common coordination patterns, i.e. equilibrium points of the dynamics. In this paper we modify the model of Schöner et al. and use it to interpret experiments on the coordination between human limbs. We consider changes in the system as a parameter is varied and focus on pattern switching: bifurcations in which an equilibrium disappears or becomes unstable and the system moves to another equilibrium point.

2. Summary of Experimental Results.

2.1. General design of experiments. In the human multilimb experiments we summarize here (see Kelso and Jeka, 1992, for additional information) a person is seated in a specially designed chair which allows her to rhythmically move her forearms, bending at the elbows, and her lower legs, bending at the knees. All movements are made in planes parallel to the median plane of the body. The position of each limb is characterized by its absolute phase modulo $2\pi$. The absolute phase $0 = 2\pi$ is assigned to the upward peak of a limb’s movement and is defined to increase at a constant rate in between upward peaks. The downward peak of a limb’s movement occurs at an absolute phase of approximately $\pi$. The relative phase $\phi$ between two limbs is defined as the difference in their absolute phases. If two limbs are in-phase ($\phi \approx 0$), both are moving up and down together, while if two limbs are anti-phase ($\phi \approx \pi$), one limb is moving down while the other is moving up. Relative phases between limbs are calculated every time a certain target limb passes through the absolute phase 0.

An experiment consists of a series of trials starting in various initial relative phase patterns. The subject is instructed to maintain the prescribed initial pattern and to cycle her limbs smoothly and continuously at a frequency set by an auditory metronome. Although instructions emphasize maintaining a one-to-one relation between the limbs and the metronome, no particular phase relationship between the metronome and the limbs is specified. The metronome frequency is systematically increased during each trial. The subject is instructed that should she feel the pattern begin to change, she should not try to resist the change, but instead perform whatever pattern seems most comfortable. (Although not done so here, subjects are capable of switching to a previously specified pattern, if so instructed; Jeka and Kelso, 1989.) All subjects were able to perform the
initial patterns after one or two practice trials. Two types of trials were conducted: two-limb trials and four-limb trials. The results below are consistent across all subjects.

2.2. Two-limb trials. The limb pair cycled during two-limb trials can be classified as either homologous, the two arms or the two legs, or nonhomologous, one arm and one leg. Nonhomologous limbs can be either ipsilateral, on the same side of the body, or contralateral, on different sides of the body. The initial relative phase patterns for two-limb trials are in-phase and anti-phase.

When subjects cycled two homologous limbs they most often maintained either the in-phase or anti-phase pattern throughout the trial as the metronome frequency increased. However, when subjects cycled two nonhomologous limbs and started in the anti-phase pattern, they almost always switched to the in-phase pattern. Figure 1 shows a typical trial with two nonhomologous limbs starting in the anti-phase pattern. The relative phase between the arm and the leg is plotted as a function of time. Metronome frequencies are indicated below the time axis. As the metronome frequency increases, the subject switches from the anti-phase pattern to the in-phase pattern and then to a phase drifting behavior. Ipsilateral limb pairs switched from the anti-phase pattern at a lower average metronome frequency than contralateral limb pairs. Switches from the in-phase pattern to the anti-phase pattern were rarely seen. At high metronome frequencies in trials with nonhomologous limbs, phase locking was usually lost and the relative phase began to wrap through a series of values. This phase drifting was generally due to the legs cycling slower than the arms.

2.3. Four-limb trials. Eight different initial relative phase patterns were used in the four-limb trials. Four of these have analogies in quadruped
locomotion, although their interpretation here in the context of human non-
weight-bearing limb coordination is necessarily different. These are the jump
(or pronk), in which all four limbs are in-phase, the bound, in which homologous
limbs are in-phase and the non-homologous limbs are anti-phase, the pace,
in which homologous limbs are anti-phase and ipsilateral limbs are in-
phase, and the trot, in which homologous limbs are anti-phase and ipsilateral
limbs are anti-phase. In the four other initial patterns, referred to as tripod
patterns, three limbs are in-phase with each other and are anti-phase with the
fourth limb. The tripod patterns will be designated with the anti-phase limb
(e.g. right arm tripod).

Figure 2 shows a histogram of switches between patterns observed in three
subjects. A switch from a pattern to itself indicates that the subject was able to
maintain the pattern during the entire trial as the metronome frequency
increased. The jump is the only pattern that was always maintained throughout
the trial. In the other extreme the trot and the bound were never maintained
throughout the trial; the trot always switched to the pace and the bound always
switched to the jump. Tripod patterns showed a variety of switching behaviors.
All four tripod patterns displayed transitions to the jump and pace, or between
homologous and limb tripod patterns. For example, the left leg tripod switched
to the jump, pace and right leg tripod, while the right arm tripod switched to the
jump, pace or left arm tripod. In some cases the tripod patterns were
maintained throughout the entire trial.

3. The model. In this section we describe a simple model of four coupled
oscillators, which aims to capture some of the more robust dynamical behavior
observed in the four-limb trials. We will use the results of the two-limb trials as
motivation. The general form of the model, oscillators with additive relative-
phase coupling, has often been used to model coupled oscillators (cf. Neu,
1979; Rand and Holmes, 1980; Cohen et al., 1982; Haken et al., 1985). The
specifics of the model are an adaptation of the model of quadruped gaits
presented in Schöner et al. (1990).

The model we consider treats each limb as an intrinsic oscillator with a stable
limit cycle. Physiological studies indicate that the muscles and joints of an
oscillating limb are constrained in such a way that the limb acts like a limit cycle
oscillator; the limb undergoes a stable oscillation and returns to the oscillation
after a perturbation (Orlovskii and Shik, 1965; Shik and Orlovskii, 1965;
Pearson, 1976; Graham, 1985). The limit cycle a limb exhibits depends on the
parameters of the system. In our experiments, the limbs are allowed to move
about only one joint (the elbow or the knee) and only in the vertical plane.

The state of each oscillator in the model is given by its absolute phase, where
the absolute phase of an uncoupled oscillator progresses linearly with time and
advances by $2\pi$ during every cycle of oscillation. Since any two phases that
differ by a multiple of $2\pi$ can be considered identical, the state space for a single oscillator is a circle. In our case of four oscillators, we let $\theta_1$, $\theta_2$, $\theta_3$ and $\theta_4$ be the absolute phases of the right arm, left arm, right leg and left leg, respectively. Phase $\theta_i = 0$ is defined to occur at the peak of each limb’s upward position. We choose a model of the form:

$$\dot{\theta}_i = \omega_i + \sum_{j=1}^{4} f_{ij}(\theta_j - \theta_i), \quad \text{for } i = 1, \ldots, 4; \quad (1)$$

where the $\dot{\theta}_i$ indicates derivatives with respect to time and $f_{ii} = 0$. The $\omega_i$ are the uncoupled angular frequencies of the limbs and the $f_{ij}$ are $2\pi$-periodic functions describing coupling from the $j$th to the $i$th oscillator. Since each $\theta_i$ lies on a circle, the state space of system (1) is the product of four circles, a four-dimensional torus.

Note that the metronome is not included in system (1). We view the metronome frequency as a parameter in the system which effects $\omega_i$ and $f_{ij}$. We do not include the absolute phase of the metronome in the model, because...
subjects are not instructed to maintain any particular phase relationship with
the metronome. In practice, the relative phases between the metronome and
the limbs are not always the same for a given pattern and do not behave
systematically during transitions between patterns.

System (1) assumes that the coupling between oscillators only depends
on their relative phases and that coupling from multiple oscillators superimpose
additively. This assumption of additive relative-phase coupling is motivated by
general principles of coupled oscillators, rather than by the details of the
multilimb system. Additive relative-phase coupling is a good quantitative
approximation for weakly coupled oscillators whose intrinsic frequencies are
close (Cohen et al., 1982; Ermentrout and Kopell, 1984), or for strongly
coupled oscillators whose interactions are appropriately dispersed throughout
the cycle (Ermentrout and Kopell, 1991). Even for systems of oscillators not
included in these cases, one expects that additive relative-phase coupling will
often be a useful qualitative description. This is particularly plausible for the
multilimb system, because the coupling between limbs is not especially strong;
it typically takes several cycles to converge onto a pattern. Also, the behavior of
two limbs is consistent with relative phases dynamics. For example, up and
down oscillations in the relative phase are not observed.

We now consider the form of the functions $f_{ij}$ in (1). Isolating two of the four
limbs gives:

$$
\dot{\theta}_i = \omega_i + f_{ij}(\theta_j - \theta_i),
\dot{\theta}_j = \omega_j + f_{ji}(\theta_i - \theta_j).
$$

Letting $\phi = \theta_i - \theta_j$ and $\Omega = \omega_i - \omega_j$, system (2) reduces to:

$$
\dot{\phi} = \Omega + f_{ij}(-\phi) - f_{ji}(\phi).
$$

Zeroes of the right hand side of equation (3) with a negative derivative
correspond to stable relative phases between the two limbs. Recall that in two-
limb trials relative phases between limbs near 0 (in-phase) or near $\pi$ (anti-
phase) are typically found. This suggests that equation (3) should take the
qualitative form of:

$$
\dot{\phi} = \Omega - a \sin(\phi) - b \sin(2\phi).
$$

Equation (4) can be obtained from (3) by taking:

$$
f_{ij}(\phi) = a_{ij} \sin(\phi) + b_{ij} \sin(2\phi),
$$

for $i, j = 1, \ldots, 4$ with $i \neq j$, and letting $a = a_{ij} + a_{ji}$ and $b = b_{ij} + b_{ji}$. We will take
equation (5) as our choice of the $f_{ij}$, although other choices are certainly
possible. For example, an even function could be added to all the $f_{ij}$. This
addition would not change the relative phase equation (4), but would change the resulting frequency of the coupled oscillators. See Kopell (1988) for further discussion of this point.

Equation (4) has been derived from specific models of weakly coupled oscillators (Rand and Holmes, 1980; Haken et al., 1985). With $\Omega=0$, it has been used as a model for two-hand coordination (Haken et al., 1985) and with $\Omega \neq 0$, as a model for hand synchronization with a metronome (Kelso et al., 1990).

Saddle-node bifurcations of (4), at which a stable fixed point and an unstable fixed point coalesce and disappear, are found by setting the right-hand side of (4) and its derivative equal to zero. This procedure yields:

$$\Omega = \sigma_2 \left( \frac{3a + \sigma_1 \sqrt{a^2 + 32b^2}}{4} \right) \sqrt{\frac{-a^2 + 16b^2 + \sigma_1 a \sqrt{a^2 + 32b^2}}{32b^2}},$$

$$\phi = \sigma_2 \cos^{-1} \left( \frac{-a + \sigma_1 \sqrt{a^2 + 32b^2}}{8b} \right);$$

where $\sigma_1, \sigma_2 = \pm 1$ (cf. Rand and Holmes, 1980). Figure 3 plots the bifurcation curves (6) in $(a/b, \Omega/b)$ parameter space for $b > 0$. Regions of in-phase, anti-phase and drifting solutions are indicated. We use the terms in-phase and anti-phase loosely to indicate solutions with $\phi$ near 0 (between $-\pi/4$ and $\pi/4$) or near $\pi$ (between $3\pi/4$ and $5\pi/4$), respectively. A drifting solution is a repetitive wrapping of $\phi$ around the circle, either in the upward or downward direction.

Having chosen the form of the $f_{ij}$, we now further constrain the behavior of system (1) by imposing left–right symmetry. Specifically, we assume that $\omega_1 = \omega_2, \omega_3 = \omega_4, f_{12} = f_{21}, f_{34} = f_{43}, f_{13} = f_{24}, f_{31} = f_{42}, f_{41} = f_{23}$ and $f_{32} = f_{43}$. Since the coupling in system (1) only depends on relative phases, we can reduce the state space from a four-dimensional torus to a three-dimensional torus by using relative phase coordinates rather than absolute phase coordinates. Of the numerous relative phases one could consider, we chose the following since they behave nicely under left–right symmetry:

$$\phi_f = \theta_1 - \theta_2,$$

$$\phi_h = \theta_3 - \theta_4,$$

$$\phi_{fh} = (\theta_1 - \theta_3) + (\theta_2 - \theta_4) = (\theta_1 - \theta_4) + (\theta_2 - \theta_3).$$

Here $\phi_f$ is the phase between the arms (front limbs), $\phi_h$ is the phase between the legs (hind limbs) and $\phi_{fh}$ is the sum of the phase between the two right limbs.
and the phase between the two left limbs. The relative phases, $\phi_{ij} = \theta_i - \theta_j$, between limbs are given in terms of the coordinate system (7) by:

$$
\phi_{12} = \phi_f, \quad \phi_{13} = \frac{1}{2} (\phi_{fh} + \phi_f - \phi_h), \quad \phi_{14} = \frac{1}{2} (\phi_{fh} + \phi_f + \phi_h),
$$

$$
\phi_{34} = \phi_h, \quad \phi_{24} = \frac{1}{2} (\phi_{fh} - \phi_f + \phi_h), \quad \phi_{23} = \frac{1}{2} (\phi_{fh} - \phi_f - \phi_h). \quad (8)
$$

The $\phi_{ij}$ as functions of $\phi_f$, $\phi_h$ and $\phi_{fh}$ in equation (8) are invariant, modulo $2\pi$, under the transformations:

$$
(\phi_f + 2\pi, \phi_h, \phi_{fh}) \rightarrow (\phi_f, \phi_h, \phi_{fh} + 2\pi),
$$

$$
(\phi_f, \phi_h + 2\pi, \phi_{fh}) \rightarrow (\phi_f, \phi_h, \phi_{fh} + 2\pi),
$$

$$
(\phi_f, \phi_h, \phi_{fh} + 4\pi) \rightarrow (\phi_f, \phi_h, \phi_{fh}). \quad (9)
$$

Therefore, we use as our state space the box \{\kappa_f \leq \phi_f \leq \kappa_f + 2\pi, \kappa_h \leq \phi_h \leq \kappa_h + 2\pi, \kappa_{fh} \leq \phi_{fh} \leq \kappa_{fh} + 4\pi\} with the sides identified by (9) to form a three-dimensional torus. The constants $\kappa_f$, $\kappa_h$ and $\kappa_{fh}$ here are arbitrary. Table 1 gives the coordinates of the eight prototypical patterns. As mentioned above, a
Table 1. Coordinates of the eight prototypical patterns

<table>
<thead>
<tr>
<th>Pattern</th>
<th>$\phi_f$</th>
<th>$\phi_h$</th>
<th>$\phi_{fh}$</th>
</tr>
</thead>
<tbody>
<tr>
<td>Jump</td>
<td>0</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>Bound</td>
<td>0</td>
<td>0</td>
<td>$2\pi$</td>
</tr>
<tr>
<td>Pace</td>
<td>$\pi$</td>
<td>$\pi$</td>
<td>0</td>
</tr>
<tr>
<td>Trot</td>
<td>$\pi$</td>
<td>$\pi$</td>
<td>$2\pi$</td>
</tr>
<tr>
<td>Right arm tripod</td>
<td>$\pi$</td>
<td>0</td>
<td>$\pi$</td>
</tr>
<tr>
<td>Left arm tripod</td>
<td>$\pi$</td>
<td>0</td>
<td>$3\pi$</td>
</tr>
<tr>
<td>Right leg tripod</td>
<td>0</td>
<td>$\pi$</td>
<td>$3\pi$</td>
</tr>
<tr>
<td>Left leg tripod</td>
<td>0</td>
<td>$\pi$</td>
<td>$\pi$</td>
</tr>
</tbody>
</table>

pattern that is close to one of the eight prototypical patterns will be referred to by the same name as its prototype.

Applying the change of coordinates (7) and imposing right–left symmetry system (1) becomes:

$$
\dot{\phi}_f = f_{12}(-\phi_f) - f_{12}(\phi_f) \\
+ f_{13}(-\phi_{fh}/2 - \phi_f/2 + \phi_h/2) - f_{13}(-\phi_{fh}/2 + \phi_f/2 - \phi_h/2) \\
+ f_{14}(-\phi_{fh}/2 - \phi_f/2 - \phi_h/2) - f_{14}(-\phi_{fh}/2 + \phi_f/2 + \phi_h/2),
$$

$$
\dot{\phi}_h = f_{34}(-\phi_h) - f_{34}(\phi_h) \\
+ f_{31}(\phi_{fh}/2 + \phi_f/2 - \phi_h/2) - f_{31}(\phi_{fh}/2 - \phi_f/2 + \phi_h/2) \\
+ f_{41}(\phi_{fh}/2 - \phi_f/2 - \phi_h/2) - f_{41}(\phi_{fh}/2 + \phi_f/2 + \phi_h/2),
$$

$$
\dot{\phi}_{fh} = 2\delta + f_{12}(\phi_f) + f_{12}(-\phi_f) - f_{34}(\phi_h) - f_{34}(-\phi_h) \\
+ f_{13}(-\phi_{fh}/2 - \phi_f/2 + \phi_h/2) + f_{13}(-\phi_{fh}/2 + \phi_f/2 - \phi_h/2) \\
- f_{31}(\phi_{fh}/2 + \phi_f/2 - \phi_h/2) - f_{31}(\phi_{fh}/2 - \phi_f/2 + \phi_h/2) \\
+ f_{14}(-\phi_{fh}/2 - \phi_f/2 - \phi_h/2) + f_{14}(-\phi_{fh}/2 + \phi_f/2 + \phi_h/2) \\
- f_{41}(\phi_{fh}/2 - \phi_f/2 - \phi_h/2) - f_{41}(\phi_{fh}/2 + \phi_f/2 + \phi_h/2),
$$

where $\delta = \omega_1 - \omega_3$. As desired, system (10) displays the left–right symmetry clearly as an invariance under the transformation $(\phi_f, \phi_h, \phi_{fh}) \rightarrow (-\phi_f, -\phi_h, \phi_{fh})$. 


4. Invariant circles. We now consider subspaces that are invariant under the flow of system (10) and attract all nearby points in the state space. The dynamics on these attracting invariant subspaces reveal much of the dynamics of the full system.

4.1. Bound-jump invariant circle. If \( \phi_f = \phi_h = 0 \), then:

\[
\begin{align*}
\dot{\phi}_f &= \dot{\phi}_h = 0, \\
\phi_{fh} &= 2\delta + 2f_{12}(0) - 2f_{34}(0) \\
&\quad + 2f_{13}(-\phi_{fh}/2) - 2f_{31}(\phi_{fh}/2) \\
&\quad + 2f_{14}(-\phi_{fh}/2) - 2f_{41}(\phi_{fh}/2), \\
&= 2\delta - 2(a_{13} + a_{31} + a_{14} + a_{41})\sin(\phi_{fh}/2) \\
&\quad - 2(b_{13} + b_{31} + b_{14} + b_{41})\sin(\phi_{fh}).
\end{align*}
\]

Therefore, the set \( \phi_f = \phi_h = 0 \) is invariant. This set, shown as a vertical line in Fig. 4, has the topology of a circle, since the top and bottom of the box in Fig. 4 are identified. To study when this invariant circle is attracting we calculate the linearization of \( \dot{\phi}_f \) and \( \dot{\phi}_h \) around the subspace:

\[
\begin{pmatrix}
\dot{\phi}_f \\
\dot{\phi}_h
\end{pmatrix} = M \begin{pmatrix}
\phi_f \\
\phi_h
\end{pmatrix},
\]

where

\[
M = \begin{pmatrix}
-2f_{12}(0) - f_{13}(-\phi_{fh}/2) - f_{14}(-\phi_{fh}/2) & f_{13}(-\phi_{fh}/2) - f_{14}(-\phi_{fh}/2) \\
-2f_{34}(0) - f_{31}(\phi_{fh}/2) - f_{41}(\phi_{fh}/2) & -2f_{34}(0) - f_{31}(\phi_{fh}/2) - f_{41}(\phi_{fh}/2)
\end{pmatrix}
\]

If:

\[
f_{12}(0) > \max_{\phi} \{|f_{13}(\phi)|, |f_{14}(\phi)|\} \quad \text{and} \quad f_{34}(0) > \max_{\phi} \{|f_{31}(\phi)|, |f_{41}(\phi)|\},
\]

then \( M_{11} + |M_{12}| < -\rho \) and \( M_{22} + |M_{21}| < -\rho \) for some \( \rho > 0 \). If \( |\phi_f| > |\phi_h| \), then \( d|\phi_f|/dt \leq M_{11}|\phi_f| + |M_{12}||\phi_h| \leq M_{11}|\phi_f| + |M_{12}||\phi_f| \leq -\rho |\phi_f| \). Similarly, if \( |\phi_h| > |\phi_f| \), then \( d|\phi_h|/dt \leq -\rho |\phi_h| \). Combining these two inequalities, we have:

\[
\frac{d}{dt} \max\{|\phi_f|, |\phi_h|\} \leq -\rho \max\{|\phi_f|, |\phi_h|\};
\]
implying that nearby trajectories approach the invariant circle exponentially fast. Therefore, inequalities (13) give sufficient conditions for the circle $\phi_f = \phi_h = 0$ to be an attracting invariant subspace.

The result above states that if the in-phase coupling of the homologous limbs is stronger than coupling between nonhomologous limbs, then when both pairs of homologous limbs start in-phase, they will remain in-phase. In this case the dynamics are constrained to lie on a circle containing the bound and the jump (see Fig. 4). Note from (11) that the flow on this circle has the same form as the flow (4) describing the coordination between two limbs. Letting $a = a_{13} + a_{31} + a_{14} + a_{41}$, $b = b_{13} + b_{31} + b_{14} + b_{41}$ and $\Omega = \delta$, Fig. 3 can now be interpreted to give regions in parameter space in which the jump (in-phase), bound (anti-phase) or drifting through the two patterns occur.

4.2. Trot–pace invariant circle. Analogous to the invariant circle $\phi_f = \phi_h = 0$ containing the bound and the jump, there is an invariant circle containing the trot and the pace. If $\phi_f = \phi_h = \pi$, then:
\[ \dot{\phi}_f = \dot{\phi}_h = 0, \]
\[ \dot{\phi}_{fh} = 2\delta + 2f_{12}(\pi) - 2f_{34}(\pi) \]
\[ + 2f_{13}(\phi_{fh}/2) + 2f_{14}(\phi_{fh}/2 + \pi) \]
\[ = 2\delta - 2(a_{13} + a_{31} - a_{14} - a_{41})\sin(\phi_{fh}/2) \]
\[ - 2(b_{13} + b_{31} + b_{14} + b_{41})\sin(\phi_{fh}). \] (14)

Sufficient conditions for the invariant circle \( \phi_f = \phi_h = \pi \) to be attracting are:

\[ f'_{12}(\pi) > \max \{|f'_{13}(\phi)|, |f'_{14}(\phi)|\} \] and

\[ f'_{34}(\pi) > \max \{|f'_{31}(\phi)|, |f'_{41}(\phi)|\}. \] (15)

Letting \( a = a_{13} + a_{31} - a_{14} - a_{41}, b = b_{13} + b_{31} + b_{14} + b_{41} \) and \( \Omega = \delta \), Fig. 3 now describes regions in parameter space in which the pace (in-phase), trot (anti-phase) or drifting through the two patterns occur. Figure 4 shows the trot–pace circle in state space.

4.3. Tripod invariant circles. Unlike the circles \( \phi_f = \phi_h = 0 \) and \( \phi_f = \phi_h = \pi \), that are invariant under the flow of system (10) for all parameter values, there are invariant circles that only exist in certain parameter regimes. In this subsection we consider an invariant circle containing the right leg tripod and the left leg tripod patterns that exist if the coupling between homologous limbs is significantly stronger than the coupling between nonhomologous limbs. We express this difference in coupling strengths by letting \( f_{ij} = eF_{ij}, a_{ij} = eA_{ij} \) and \( b_{ij} = eB_{ij} \) for \( ij \in \{13, 31, 14, 41\} \), where \( 0 < e \ll 1 \). The coupling functions \( f_{12} \) and \( f_{34} \) remain of the order 1.

If the arms are stably in-phase \( (\phi_f = 0, f'_{12}(0) > 0) \), the legs are stably anti-phase \( (\phi_f = \pi, f'_{34}(\pi) > 0) \) and all connections between the arms and the legs are severed \( (e = 0) \), then system (10) reduces to:

\[ \dot{\phi}_f = \dot{\phi}_h = 0, \]
\[ \dot{\phi}_{fh} = 2\delta + 2f_{12}(0) - 2f_{34}(\pi) = 2\delta. \] (16)

In this limiting case the circle \( \{\phi_f = 0, \phi_h = \pi\} \) containing both leg tripods is invariant and attracting. This attracting invariant circle will persist if \( e \) is sufficiently small, although in general its shape will become deformed (Hirsch et al., 1977).

We now consider the flow on the invariant circle. Using \( \phi_f = O(\varepsilon) \) and \( \phi_h = \pi + O(\varepsilon) \), the expression for \( \dot{\phi}_{fh} \) in (10) becomes:
\[
\dot{\phi}_{fh} = 2\delta + 2f_{12}(0) - 2f_{34}(\phi) \\
+ \varepsilon F_{13}\left(-\frac{1}{2} \phi_{fh} + \frac{\pi}{2}\right) + \varepsilon F_{13}\left(-\frac{1}{2} \phi_{fh} - \frac{\pi}{2}\right) \\
- \varepsilon F_{31}\left(\frac{1}{2} \phi_{fh} - \frac{\pi}{2}\right) - \varepsilon F_{31}\left(\frac{1}{2} \phi_{fh} + \frac{\pi}{2}\right) \\
+ \varepsilon F_{14}\left(-\frac{1}{2} \phi_{fh} - \frac{\pi}{2}\right) + \varepsilon F_{14}\left(-\frac{1}{2} \phi_{fh} + \frac{\pi}{2}\right) \\
- \varepsilon F_{41}\left(\frac{1}{2} \phi_{fh} - \frac{\pi}{2}\right) - \varepsilon F_{41}\left(\frac{1}{2} \phi_{fh} + \frac{\pi}{2}\right) + O(\varepsilon^2). \\
\]

We note from (17) that phase locking is only possible if \(\delta = O(\varepsilon)\). Therefore, we let \(\delta = \varepsilon \Delta\) and write the flow on the invariant circle as:

\[
\dot{\phi}_{fh} = \varepsilon[2\Delta + 2(B_{13} + B_{31} + B_{14} + B_{41})\sin(\phi_{fh})] + O(\varepsilon^2).
\]

The bifurcation diagram for (18) is given by Fig. 3, with \(a = 0, b = B_{13} + B_{31} + B_{14} + B_{41} + O(\varepsilon)\) and \(\Omega = \Delta\). Arbitrarily, we let in-phase refer to the right leg tripod pattern and anti-phase to the left leg tripod pattern. When \(\Delta = 0\) the flow (18) has stable fix points at \(\phi_{fh} = \pi + O(\varepsilon)\) and \(\phi_{fh} = 3\pi + O(\varepsilon)\), corresponding to the left leg tripod and the right leg tripod, respectively (see Table 1). As \(\Delta\) passes upwards through \(B_{13} + B_{31} + B_{14} + B_{41} + O(\varepsilon)\), both tripod patterns cease to be fixed points simultaneously and upward drifting begins.

Analogous to the leg tripod circle described above, there is an invariant circle containing the arm tripod patterns (see Fig. 4). The flow on the arm tripod circle has the same form as (18).

5. Discussion. In this section we compare the behavior of the model to the behavior of the experimental system. Specifically, we examine whether the invariant circles of the model are reflected in the dynamics of the limb movements of the subjects and, if so, whether the direction of switches between two patterns on the same circle can be interpreted by the model.

We saw above that the model has four attracting invariant circles (bound–jump, trot–pace, arm tripod and leg tripod), if the coupling between homologous limbs is sufficiently stronger than the coupling between non-homologous limbs. Even though Fig. 2 shows that switches are observed between invariant circles (e.g. right arm tripod to jump), the majority of
transitions are observed within a circle. In particular, there are no switches out
of the bound–jump circle, all switches from the trot go to the pace and a number
of switches occur between tripod patterns on the same circle.

Figure 5 shows trajectories in state space of one subject. Five trials starting
in each of the eight patterns are plotted. There is a strong indication of the
bound–jump circle and the leg tripod circle, as well as some evidence of the
trot–pace circle (cf. Fig. 4). Although there are trajectories between circles,
most trajectories between patterns lie near the circles of the model. The circles
most evident vary with subject. Only the bound–jump circle was clearly seen in
all three subjects.

We now restrict our attention to switches between patterns on the same
circle. Recall from Fig. 2 that there are switches in both directions on the two
tripod circles, but switches only occur from bound to jump on the bound–jump
circle and only from trot to pace on the trot–pace circle. Our goal is to interpret
these results based on our knowledge of two-limb coordination.

If we consider coordination between the two limbs $i$ and $j$ with $i<j$, then

![Figure 5. Phase trajectories of the subject GP from all the experimental four-limb trials. Dotted lines connect measured three-dimensional points of the relative phase used to characterize the four-limb patterns. Note that trajectories accumulate close to the invariant circles from the model.](image-url)
Fig. 3 is the bifurcation diagram for their dynamics, where \( a = a_{ij} + a_{ji} \), \( b = b_{ij} + b_{ji} > 0 \) and \( \Omega = \omega_1 - \omega_j \). During a trial we imagine the point \((a/b, \Omega/b)\) in parameter space varying as the metronome frequency is increased. The experimental two-limb data suggest the following dependence of the parameters on metronome frequency. For two homologous limbs \( \Omega = 0 \) and \((a/b, \Omega/b)\) remains within the region of Fig. 3, in which both the in-phase and anti-phase patterns are stable. For two nonhomologous limbs \( \Omega = \omega_1 - \omega_3 \) and \((a/b, \Omega/b)\) moves from the region of bistability, through the region in which only the in-phase pattern is stable and into the region of upward drifting. Based on this description we assume that \( a > 0 \) and \( \omega_1 - \omega_3 \) is an increasing function of metronome frequency. Although not strictly necessary for the discussion that follows, for simplicity we also assume that \( a \) and \( b \) do not vary with metronome frequency. Not that under these assumptions, the size of \( a \) determines the frequency at which the anti-phase pattern is lost. If \( a \) is increased the anti-phase pattern is lost at a lower metronome frequency.

The bifurcation diagram for the dynamics on the bound-jump circle is given by Fig. 3 with \( a = a_{13} + a_{31} + a_{14} + a_{41} \), \( b = b_{13} + b_{31} + b_{14} + b_{41} \) and \( \Omega = \omega_1 - \omega_3 \). Here, in-phase refers to the jump and anti-phase refers to the bound. Since we are assuming that \( a_{13} + a_{31} > 0 \) and \( a_{14} + a_{41} > 0 \) based on two-limb dynamics, we have \( a > 0 \). Therefore, as \( \Omega \) increases with metronome frequency the model suggests that the bound should switch to the jump. This is the direction of switches found in the four-limb trials.

The bifurcation diagram for the dynamics on a tripod circle is given by Fig. 3 with \( a = 0 \), \( b_{13} + b_{31} + b_{14} + b_{41} = \varepsilon b + O(\varepsilon^2) \) and \( \omega_1 - \omega_3 = \varepsilon \Omega \), where \( \varepsilon \ll 1 \) is the ratio between nonhomologous coupling strength and homologous coupling strength. In-phase and anti-phase refer arbitrarily to the two tripod patterns on the circle. Since parameters are constrained to the vertical axis of Fig. 3, both tripod patterns cease to be fixed points simultaneously as \( \Omega \) increases. Instead the solution continuously wraps around the circle with \( \phi_{fh} \) increasing, slowing each time it passes through one of the two tripod patterns. This description is consistent with the experimental results, except that fluctuations not in the model appear to cause premature switches between tripod patterns on the same circle. Elsewhere, fluctuations have been explicitly taken into account in theoretical and empirical studies of interlimb coordination (Schöner et al., 1986; Kelso et al., 1986), but we do not pursue this further here.

Finally, the bifurcation diagram for the dynamics on the trot-pace circle is given by Fig. 3, with \( a = a_{13} + a_{13} + a_{14} - a_{41} \), \( b = b_{13} + b_{31} + b_{14} + b_{41} \) and \( \Omega = \omega_1 - \omega_3 \). In-phase refers to the pace and anti-phase refers to the trot. As with the bound-jump circle, we assume that \( a_{13} + a_{31} > 0 \) and \( a_{14} + a_{41} > 0 \). However, now these inequalities do not determine the sign of \( a \). Recalling from the two-limb trials that ipsilateral nonhomologous limbs lose the anti-phase
pattern at a lower average metronome frequency than contralateral nonhomologous limbs, we assume that $a_{13} + a_{31} < a_{14} + a_{41}$. Therefore, $a > 0$, which in turn implies that the trot should switch to the pace as the metronome frequency increases. This direction of pattern switching matches the experimental four-limb data.

In summary, much of the behavior of the experimental multilimb system can be interpreted by the model. The experimental trajectories of the relative phase usually lie near the invariant circles of the model (compare Fig. 4 and 5) and the direction of switches between two patterns on the same circle is consistent with data from two-limb trials.

There is much general interest now in phase and frequency synchronization in neurobiological systems. Such phenomena have been observed in many systems and at different levels. The present approach interprets switches in the pattern of coordination between limbs as bifurcations in a dynamical system. Some of the mathematical concepts employed (symmetry, invariant subspaces, etc.) may be generally useful in the analysis of other systems. At the same time our approach affords further experimental explorations, for example, of transition pathways and preferred routes among multiple patterns in the present experimental model system.

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LITERATURE


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